EBOOK

THE RISK MANAGEMENT + DESIGN CONTROLS CONNECTION: WHAT DEVICE MAKERS NEED TO KNOW

JON SPEER, FOUNDER & VP OF QA/RA GREENLIGHT.GURU
THE RISK MANAGEMENT + DESIGN CONTROLS CONNECTION: WHAT DEVICE MAKERS NEED TO KNOW

TABLE OF CONTENTS

2. Intended Use & User Needs
9. Verification, Validation, & Risk Controls
17. Using Design Reviews Effectively
INTENDED USE & USER NEEDS

Medical devices are intended to save and improve quality of life.

I like the ISO 13485:2003 definition of a medical device: “Any instrument, apparatus, implement, machine, appliance, implant, in vitro reagent or calibrator, software, material or other similar or related article, intended by the manufacturer to be used, alone or in combination, for human beings for one or more of the specific purpose(s) of:

- diagnosis, prevention, monitoring, treatment or alleviation of disease
- diagnosis, monitoring, treatment, alleviation of or compensation for an injury
- investigation, replacement, modification, or support of the anatomy or of a physiological process
- supporting or sustaining life
- control of conception
- disinfection of medical devices
- providing information for medical purposes by means of in vitro examination of specimens derived from the human body”

A medical device should address a specific patient and clinical need, defined by manufacturers in an intended use statement. Intended use is key to your product development and risk management efforts, as well as critical to your regulatory strategy, helping to determine classification and go-to-market strategy.
This is really where a medical device’s journey begins. Design controls and risk management should flow and blend together, and it’s important to establish this flow early in product development. Intended use is a gateway to user needs, design & development plan, design inputs, risk management plan, hazards, hazardous situations, and foreseeable sequence of events.

**INTENDED USE HELPS DEFINE USER NEEDS**

Intended use defines the purpose of a medical device. User needs are then derived and defined from the intended use to describe:

– *Who will use this device?*
– How will the user and patient interact with the device?
– What type of procedures will the device be used for?
– What type of environment will the device be used in?
– When will the device be used?
– Is the device used one time, or over and over?
– What other products will the device interact and interface with?

I’ve talked before about the importance of user needs in the design controls process. User needs start the “waterfall,” and design validation closes the process, cycling back to user needs.
APPLY INTENDED USE TO YOUR DESIGN & DEVELOPMENT PLAN

Intended use and user needs define the scope of a project, and they are instrumental in establishing a design & development plan. Such a plan needs to define:

- Design & development stages and activities
- Who is responsible for design & development activities
- Resources required, such as project team members and key vendors
- Timing of design reviews

The plan is not a “one and done” and needs to be revisited and updated throughout the project.

DESIGN INPUTS BUILD ON USER NEEDS

To define design inputs for your medical device, you need to understand user needs. I’m guessing you can cite several projects where you were able to define design inputs, but there may not have been any defined user needs. Actually, there were user needs — they just might not have been documented, and this can be an issue.

User needs should always be defined and documented. Doing so helps to define design inputs. Otherwise, you might have to guess and fill in the blanks. When this latter approach is taken, you can progress far into product development before realizing your device has not addressed key aspects from the end-user
and patient perspective. It’s even possible to launch a device into the market and discover later, through product complaints, that you overlooked some user needs.

Intended use usually comprises a few sentences that describe what a product is supposed to do. User needs are a series of statements that further describe the intended use. It is okay if your user needs are somewhat vague and ambiguous.

For example, a user need may state something like “the product should be easy to use.” This is where design inputs come into play. They describe and define “easy to use” in clear, objective terms. Think of the design inputs as a contract — a product developer should be able to reference this contract during design and development of the product.

**INTENDED USE GUIDES RISK MANAGEMENT PLANNING**

One of the first steps involved in medical device risk management is establishing a risk management plan, which describes risk management activities throughout the product lifecycle. Roles and responsibilities, as well as the risk management team, are defined. Intended use is important because it helps to establish the scope to which risk management activities will be necessary.

The risk management plan also includes criteria for your medical device’s risk acceptability, which should be commensurate with the intended use. Like the design & development plan, a risk management plan is continually evolving throughout the product lifecycle.
HAZARDS, HAZARDOUS SITUATIONS, FORESEEABLE SEQUENCE OF EVENTS BASED ON INTENDED USE

Risk management also includes risk analysis and risk evaluation — described in Understanding ISO 14971 Medical Device Risk Management. Risk analysis and risk evaluation make up what is known as a risk assessment.

**Snap shot of risk analysis and risk evaluation from ISO 14971:2007.**

A risk assessment, based on a device’s intended use, determines the possible hazards, hazardous situations, and foreseeable sequence of events related
to your medical device. A hazard is a potential source of harm, while a hazardous situation is a circumstance in which people, property, or the environment are exposed to one or more hazard(s). The foreseeable sequence of events lays out the steps required for a hazardous situation to result.

**THE CONNECTION BETWEEN DESIGN CONTROLS AND RISK MANAGEMENT**

Just as intended use plays a vital role in design control and risk management, design control and risk management are vital to one another. Some companies treat design controls and risk management as related but separate processes, not realizing the close connection between user needs, design inputs, hazards, and hazardous situations.

Intended use leads to user needs, which lead to design inputs — the “contract” by which medical devices are designed and developed. Intended use also helps define the scope of a design & development plan, as well as the scope of a risk management plan. All of this information is used to determine hazards, hazardous situations, and foreseeable sequence of events.

As I stated at the beginning of this article, medical devices are intended to save and improve quality of life. Following sound design controls and risk management processes helps ensure that the devices you design, develop, manufacture, and sell are as safe and effective as possible.
The previous article in this series addressed design control and risk management connections through intended use and user needs — specifically, how these items are key to identifying hazards, hazardous situations, and foreseeable sequence of events.

To recap, intended use leads to user needs, which lead to design inputs. Think of design inputs as a “contract” by which medical devices are designed and developed. Intended use also helps define the scope of a design & development plan, as well as the scope of a risk management plan.

Let me also remind you of the high-level risk management process overview defined in ISO 14971:
7 **Risk Control**

Use Risk Controls to reduce risks to acceptable levels:

8 **Evaluation Of Overall Risk Acceptability**

Evaluate risk of the product in its entirety.

- Is the risk level acceptable?
- Do the benefits outweigh the potential risks?

9 **Risk Management Report**

Carry out a risk management review and prepare a risk management report before sending your device to commercial production.

10 **Production And Post-production Information**

Internal audits, CAPAs, complaints, customer feedback and non-conforming material all ‘feed’ into the risk management process.

Risk management is a total product lifecycle process.
Here, I’ll continue the journey of demonstrating how design controls and risk management should flow seamlessly back and forth to improve safety and reduce risks associated with medical devices, tying in the connections that design inputs, design outputs, design verification, and design validation have with risk controls.

From the perspective of risk management, you have estimated the risks of each hazardous situation by determining severity of potential harm and its probability of occurrence.

You established risk acceptability criteria earlier, during the risk management planning phase of product development. Chances are, you have some type of risk acceptability matrix or chart where you have defined regions of both acceptable and unacceptable risks.

<table>
<thead>
<tr>
<th>Frequent</th>
<th>LOW</th>
<th>MEDIUM</th>
<th>HIGH</th>
<th>HIGH</th>
<th>HIGH</th>
</tr>
</thead>
<tbody>
<tr>
<td>Probable</td>
<td>LOW</td>
<td>MEDIUM</td>
<td>MEDIUM</td>
<td>HIGH</td>
<td>HIGH</td>
</tr>
<tr>
<td>Occasional</td>
<td>LOW</td>
<td>LOW</td>
<td>MEDIUM</td>
<td>MEDIUM</td>
<td>HIGH</td>
</tr>
<tr>
<td>Remote</td>
<td>LOW</td>
<td>LOW</td>
<td>LOW</td>
<td>MEDIUM</td>
<td>HIGH</td>
</tr>
<tr>
<td>Improbable</td>
<td>LOW</td>
<td>LOW</td>
<td>LOW</td>
<td>LOW</td>
<td>MEDIUM</td>
</tr>
<tr>
<td></td>
<td>Negligible</td>
<td>Minor</td>
<td>Serious</td>
<td>Critical</td>
<td>Catastrophic</td>
</tr>
</tbody>
</table>

Based on the risk acceptability criteria you have established, there is one significant question you need to answer at this stage: Is risk reduction necessary? If you have made the design controls and risk management connection, then the answer to this question will be a driving force for the next several stages of your medical device product development.
**ALARP VS ALAP**

Depending on where in the world you are selling medical devices, the decisions driving risk reduction can take on different meanings.

Specifically, for Europe, EN ISO 14971:2012 indicates that all risks must be reduced “as low as possible” (ALAP). If you are following ISO 14971:2007 (basically, everywhere except EU), then all unacceptable risks should be reduced to acceptable status, or to “as low as reasonably practicable” (ALARP). By the same token, risks initially in the ALARP “zone” should ideally be reduced, as well.

**THE RISK CONTROL “PHASE”**

When you have identified hazardous situations requiring risk reduction, you enter the risk control phase of the risk management process. According to ISO 14971, risk control is the process in which decisions are made and measures implemented by which risks are reduced to, or maintained within, specified levels.

---

Click to see the full infographic on the next page
Use Risk Controls to reduce risks to acceptable levels:

- **Risk Control Measure Required?**
  - No
  - Yes

- **Does Residual Risk Level Require Risk Benefit Analysis?**
  - No
  - Yes

- **Risk Benefit Analysis**
  - Yes
  - No

- **Do Benefits Outweigh Risks?**
  - Yes
  - No

- **Risk is Acceptable**
  - Yes
  - No

- **Risk is Unacceptable**
  - Yes
  - No

**Establish level of Residual Risk** (Low, Medium, High)

**Design**
- Output
- Verification
- Validation

**Documents**
- Output
- Verification
- Validation

**Use Risk Controls to reduce risks to acceptable levels:**
RISK CONTROL — CONSIDERING YOUR OPTIONS

In order to reduce risks to acceptable levels, you need to identify possible options — risk control measures — that are appropriate and substantial. There are three basic types, or levels, of risk controls you should consider, listed here in order of priority:

1. **Inherent safety by design** — Ensure that the design of the medical device reduces and/or eliminates the probability of harmful occurrences altogether.

2. **Protective measures in the medical device and/or manufacturing process** — Examples of this could include redundant features, safety mechanisms, etc., with the intent to reduce the occurrence of harm.

3. **Information for safety** — This category of risk controls — which includes labeling, instructions for use, training materials, and the like — is largely regarded as least effective, so much so that EN ISO 14971:2012 does not allow you to use this as a means for risk control because information for safety is a general requirement of medical devices.

RISK CONTROLS AND THE DESIGN CONTROLS CONNECTION

As you can see, there is a strong connection the levels of risk control measures and design controls.
When you identify risk control measures, these items can drive changes and revisions to your design inputs. Perhaps your design inputs can be better clarified and stated. Or, perhaps you need to include additional design inputs.

Design outputs, too, can be significantly influenced by your risk control measures. Remember that the design outputs established during medical device product development serve as the preliminary device master record (DMR) for the product. In other words, the design outputs are the “recipe” for your medical device. Risk control measures relating to design outputs could lead to adding new safety features into your product and providing more clarity and definition in design output documents.

**KEY TIP:**

I like to do a first pass through risk analysis, risk evaluation, and risk controls after I have my user needs and design inputs defined, and **BEFORE** doing too much work on my design outputs, design verification, and design validation.

Why? I want to know what my initial risk levels are before creating overly complicated drawings and specifications, and before conducting expensive — and maybe unnecessary — verification and validation (V&V) testing.

Identifying risk control measures should help you define what type of design verification activities will be necessary to demonstrate that your design outputs meet your design inputs, and to prove your medical device is safe. Design verification activities are also instrumental in providing some objective evidence to support probability of events that could lead to harm.
As with design verification, risk control measures can also help shape what type of design validation will be necessary to prove the product addresses user needs. Design validation can serve as a means to determine if hazards and hazardous situations are likely during intended use. Results of design verification and design validation will be influential when estimating and evaluating residual risks.

**RESIDUAL RISK ACCEPTABILITY**

After identifying all risk control measures and implementing them, the next step is to evaluate and estimate the residual risks: Did you successfully reduce risks to acceptable levels? If not, consider additional risk controls.

Or, maybe you can conduct a risk/benefit analysis where you evaluate and weigh the medical benefits your device provides against the risks. If you choose this path, document the explanation. Also, note that risk/benefit analysis is another area where EN ISO 14971:2012 differs. If you have devices in EU, then you need to document a risk/benefit analysis for all of your risks.

Did your risk controls introduce new hazards and hazardous situations? If so, analyze, evaluate, and estimate the risks from these new scenarios.

**CONCLUSIONS**

Risk control measures are the key to identifying ways to mitigate and reduce your product’s risks to acceptable levels. Risk controls provide a means to help
you develop your medical device “recipe” through design outputs, to prove these outputs meet design inputs via design verifications, and to prove your medical device meets end user needs.

As I have stated before, medical devices are intended to save and improve quality of life.

Following sound design controls and risk management processes helps ensure that the devices you design, develop, manufacture, and sell are as safe and effective as possible.

USING DESIGN REVIEWS EFFECTIVELY

Design controls and risk management are key to the success of a medical device, in that they demonstrate that your product is safe and effective for its intended uses. Furthermore, there is a strong, complementary relationship between design controls and risk management, something we have discussed in this series’ previous installments.

Part one explored design control and risk management connections through intended use and user needs, while part two connected risk controls to design outputs, design verification, and design validation. In this installment, I will discuss best practices regarding design reviews, and how to incorporate risk management as a critical element helping to drive decisions.
DESIGN REVIEWS — BREAKING DOWN THE REQUIREMENTS

I like to start with the good ol’ design controls “waterfall” diagram to show how design reviews fit into the medical device product development paradigm:

Design reviews are intended to encompass all aspects of design controls. Yes, that’s correct — all design control efforts should be included as part of a design review throughout the product development process. Consider what FDA 21 CFR part 820.30(e) and ISO 13485:2003 section 7.3.4 state about design reviews:
820.30(e) — Design review —

Each manufacturer shall establish and maintain procedures to ensure that formal documented reviews of the design results are planned and conducted at appropriate stages of the device’s design development.

The procedures shall ensure that participants at each design review include representatives of all functions concerned with the design stage being reviewed and an individual(s) who does not have direct responsibility for the design stage being reviewed, as well as any specialists needed. The results of a design review, including identification of the design, the date, and the individual(s) performing the review, shall be documented in the design history file (the DHF).

ISO 13485:2003 — section 7.3.4 —

Design and development review — At suitable stages, systematic reviews of design and development shall be performed in accordance with planned arrangements (see 7.3.1):

a) to evaluate the ability of the results of design and development to meet requirements, and

b) to identify any problems and propose necessary actions.

Participants in such reviews shall include representatives of functions concerned with the design and development stage(s) being reviewed, as well as other specialist personnel (see 5.5.1 and 6.2.1).

The key take-home points for design reviews are that they must:

• Be planned at suitable and appropriate stages during product development
DESIGN REVIEW VS PHASE REVIEW

Taken literally, the waterfall diagram suggests that design controls and subsequent design reviews follow a serial, or linear, progression.

Use of this methodology to manage product development projects is common in, but not unique to, the medical device industry. The “phase-gate model” (branded as Stage-Gate by Drs. Robert Cooper and Scott Edgett) bears a striking resemblance to the design control stages identified in the waterfall.

The basic premise is that each phase, or stage, is defined with minimum criteria and milestones. Before moving to the next phase, you need to satisfy that the criteria have been met, and the way to do so is via formal phase review. I bring this up for one primary reason. The medical device design controls process is more or less a phase gate approach, but with a slight twist.

The purpose of a phase review is to make a business decision — whether or not to continue funding a project, with dollars and resources, into the next phase of product development.

Design reviews serve a similar purpose, but dollars and resources are not the key metrics to monitor. With a medical device, the purpose at each stage is to
demonstrate an acceptable level of safety and efficacy before continuing to the next stage. Design reviews are a mechanism used to assess and document these decisions.

It’s worth noting that there are ongoing debates on whether design reviews and phase reviews both are required for medical device product development. One point of view suggests that these should be separate events: Phase reviews analyze business decisions; Design reviews analyze design controls. The other point of view suggests that blending phase reviews with design reviews is perfectly fine.

Based on my 17+ years of experience with medical device product development, I recommend the latter approach. Do yourself a favor: Combine phase reviews and design reviews into a single meeting. Capture the design controls details on a design review form and other nondesign control items in separate notes. We all have too many meetings as it is. Try to simplify things a bit when you can.

MUST MEDICAL DEVICE PRODUCT DEVELOPMENT BE LINEAR?

Conventional wisdom suggests that linear product development processes are generally less risky (in a project sense of the word), versus processes that allow parallel activities. The en vogue product development practices involve lean and agile approaches, though, and you definitely can utilize such approaches in medical device product development.
But there are a few medical device design control absolutes that must occur and be documented:

1. A design output must include or make reference to acceptance criteria.

2. Design verification must demonstrate that design outputs meet design inputs. A design verification can only be conducted after design output/design input relationships have been established.

3. Design validation must demonstrate that a product meets user needs. A design validation can only be conducted after product and user needs are defined.

4. Design validation requires products to utilize production

LINKING RISK MANAGEMENT TO DESIGN REVIEWS

Again, the primary purpose of both risk management and design controls is to ensure that your product is safe and effective for its intended uses. Demonstrating this requires objective evidence documented in a design history file and a risk management file.

Blending design controls and risk management, rather than treating them as entirely independent workflows, will improve your medical devices, and one way to bring these practices together is via design reviews.

As noted, you need to conduct design reviews at appropriate stages during design and development. I’ll let you decide on how often and how many. But since you are asking, my advice is to conduct a minimum of five design reviews, one at each of these stages: user needs, design inputs, design outputs, design verification, and design validation. Why? You need to show with objective
evidence (i.e., documentation) that all design controls have been part of design reviews. The simplest and cleanest way to do so is by having separate design reviews for each of the major design control elements.

And, at each and every one of your design reviews, risk management should be the centerpiece of the event. Use risk management as a tool, rather than a checkbox activity. Use your ISO 14971-compliant approaches to drive risk-based decision-making as a practice within your medical device product development efforts. Identify where your product risks are, and discuss how to mitigate and control those risks via design controls; document these discussions as part of design reviews.

Understanding how to blend design controls and risk management efforts into a continuous stream will bring purpose and meaning to your product development efforts.

As regulatory bodies around the world harmonize their concepts of “risk-based approaches,” and tout the importance of complying with ISO 14971, you must evolve your own internal practices, as well.
THE RISK MANAGEMENT + DESIGN CONTROLS CONNECTION: WHAT DEVICE MAKERS NEED TO KNOW